

# PREDICTING PERFORMANCE IMPROVEMENT UNDER CUSTOMIZED HAPTIC ASSISTANCE

# HUR (Human Rehabilitation) Group Attp://hurgroup.net

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# INTRODUCTION

#### Motivation

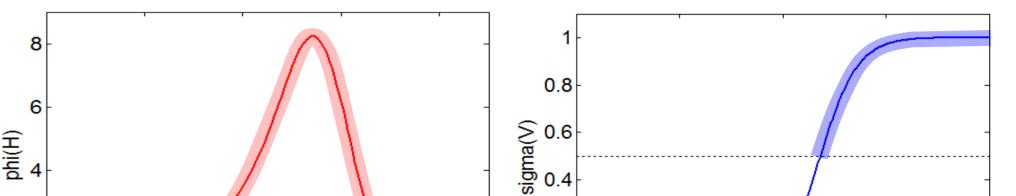
- For haptic assistive control, various approaches to adapting the assistance level to the user's skill level have been presented.
- Although there have been ample

#### **Data Collection**

- Completion time, sampling time, task#, trial#, # of successes, # of fails, vehicle's positions and heading direction were recorded from the start line to the finish line.
- Each condition was repeated 3 times. The sequence of the tasks was randomized.
- Sampling frequency was 60Hz.

 $\sigma(V) = \left(1 + e^{-k(V-V_0)}\right)^{-1}$  where  $V_0$  is a bias

and  $\varphi(H)$  was estimated by using a kernel density estimation (see Fig. 3).



considerations about adjusting the assistance levels, the efficacy of these methods on user's performance has still remained inconclusive.

#### Objectives

 To predict the potential improvement of user's performance under a customized haptic assistance for each user.

## Approach

- Represent the temporospatial characteristics of a controlled path demonstrated by a user under no-assistance with two metrics: *variability* and *Hurst exponent*.
- With the user's data under customized assistance, we will train a classifier function to distinguish the improved users and unimproved users by using machine learning techniques.

#### METHODS

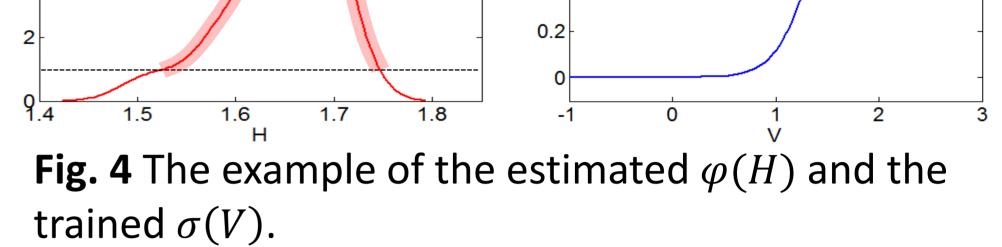
# Representing the Temporospatial Characteristics of a Controlled Path

- After completing all sessions, subjects' performances under no assistance and customized haptics were examine in terms of variability (temporal) and Hurst exponent (spatial).
- First, the variability was computed as a summed standard deviation of mean completion time for all scenarios

$$V = \sum_{i=1}^{4} std\left(mean\left(\sum_{j=1}^{3} T_{i,j}\right)\right)$$

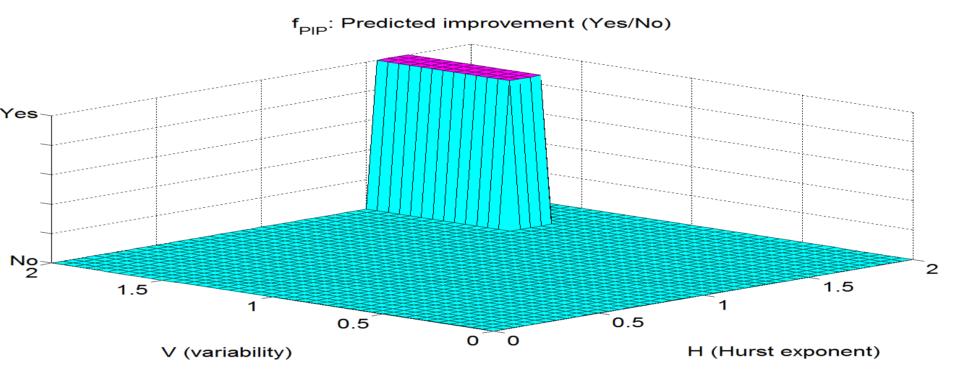
where *i* and *j* are indices for scenario and repetition, respectively.

Next, Hurst exponent, *H*, was obtained from detrended fluctuation analysis (DFA) which tells us the slow/fast varying characteristics of time course data (see Fig. 2) [2]. *H* is the



• Finally, from the trained  $\sigma(V)$  and the estimated  $\varphi(H)$ , the performance improvement predictor function,  $f_{\text{PIP}}$ , could be defined as

$$f_{\text{PIP}}(\sigma(V), \varphi(H)) = \begin{cases} \text{yes, if } \sigma(V) \ge 0.5 \land \varphi(H) \ge 1\\ \text{no, otherwise} \end{cases}$$



**Fig. 4** The example of  $f_{PIP}$  from  $\varphi(H)$  and  $\sigma(V)$ .

#### Subjects

39 healthy young adults (31 male, 8 female, age=20-35) participated in this study.

**Procedures** (For more information see [1])

- Subjects were seated at 1.5m away from a 105cm-by-81cm screen
- A modified version of Novint Falcon was used as 2D haptic interface (Fig. 1).
- Experiments consisted of two separate sessions: the first session for obtaining the baseline data and the second session for identifying the effect of customized haptic feedback based on the baseline data.
- For both sessions, the subjects were asked to drive a virtual vehicle along four roads each of which had a difference radius of curvature and obstacles.

estimated power-law exponent of a scale invariant structure of a signal X(t), which is

 $X(ct) = c^H X(t)$ 

Consequently, each subject was associated with two metrics as either *subject#*:{V, H,1} or *subject#*:{V, H,0} for improved or nonimproved subjects, respectively.

### **Define a Performance Improvement Predictor** (PIP) Function

- From the associated data above, we randomly selected 80 percent of improved subjects (label: 1) and non-improved subjects (label: 0) and set them as a training set.
- A logistic sigmoid function, σ(V), was trained to yield 1 for the improved subjects and 0 for the non-improved subjects:

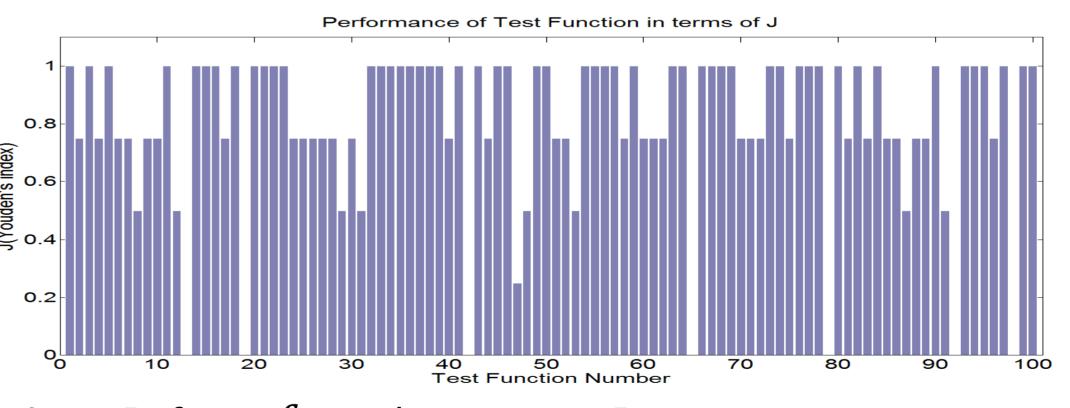
#### distance from the SCT to RT

# **RESULTS AND DISCUSSION**

- First, f<sub>PIP</sub> was generated 100 times from the randomly selected a training set, then it was validated by a test set.
- To show the accuracy of f<sub>PIP</sub>, Youden's index
   J was used [3]

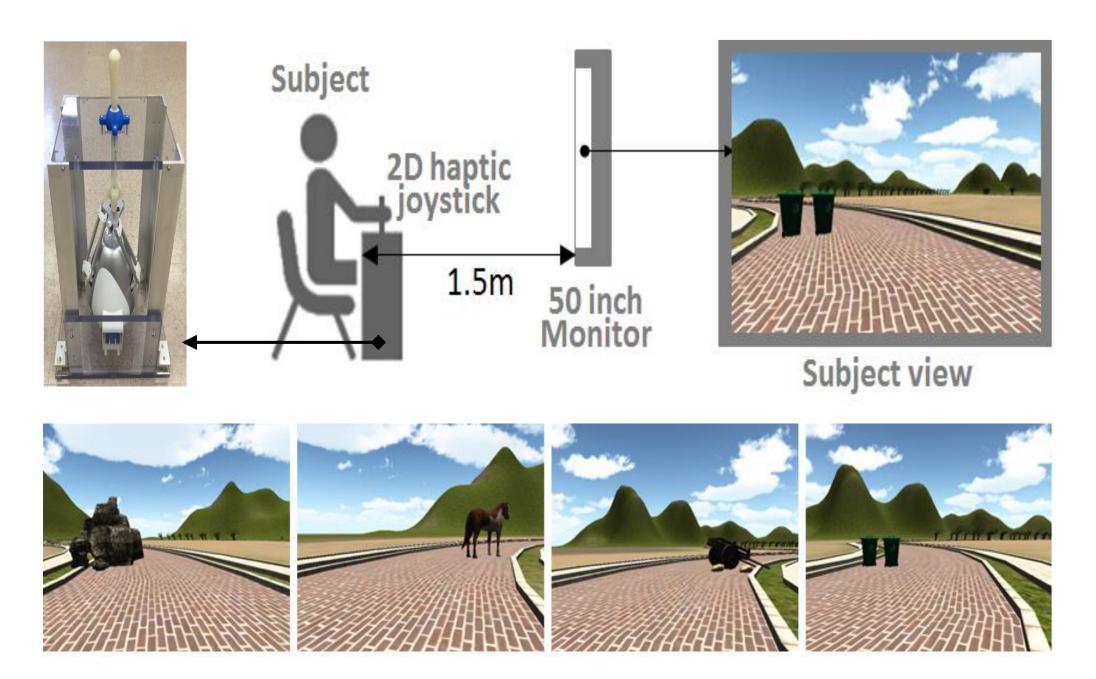
# J = sensitivity + specificity - 1

• The average of J from the 100  $f_{\rm PIP}$  was 0.803.

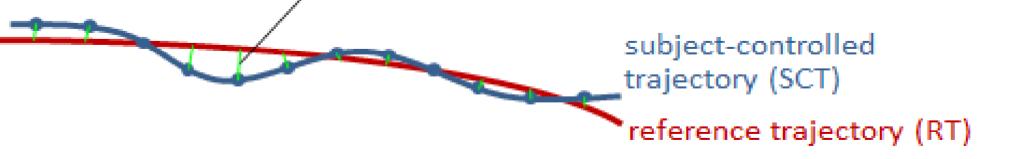


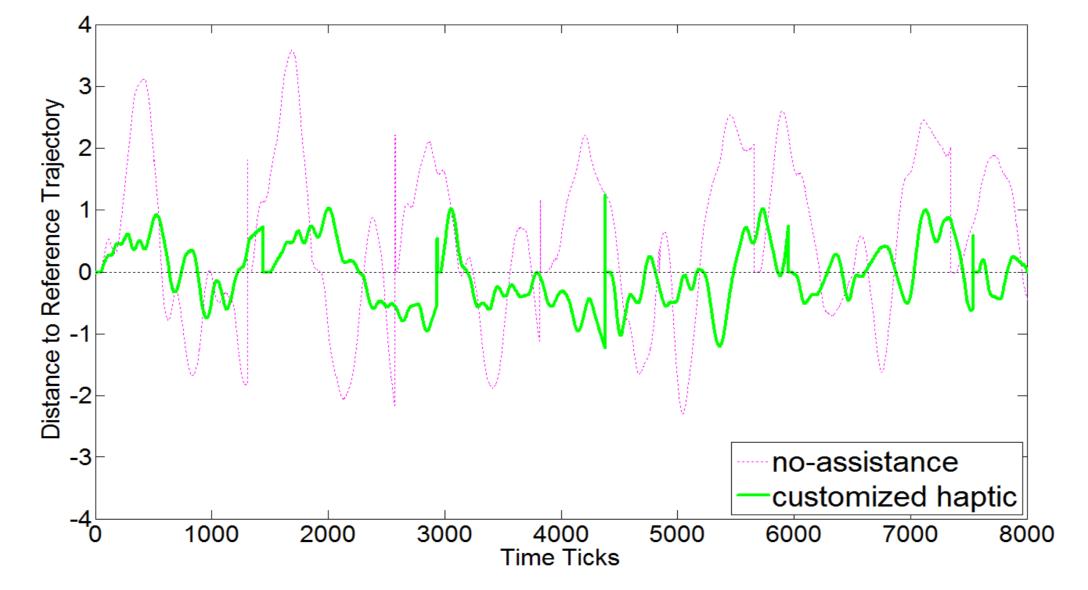
**Fig. 5** J of 100  $f_{\text{PIP}}$ . The average J is 0.803.

 Subjects were instructed to drive the vehicle as fast and safe as possible.



**Fig. 1** A virtual power-wheelchair simulator for the experiment (top) and four different scenarios (bottom).





**Fig. 2** The reference path is employed as a baseline, and the distances from the reference path under no-assistance (magenta-dotted-thin) and the customized haptic (green-solid-thick) are depicted (bottom).

#### CONCLUSION

- The temporospatial characteristics of a wheelchair path controlled by subjects were expressed in terms of variability and Hurst exponent.
- The defined f<sub>PIP</sub> can be used to predict the performance improvement with the subject-specific customized haptic feedback.

#### References

[1] Yoon H. and Hur P., American Society of Biomechanics, 2015.

[2] Kantelhardt J. W. et al., Physica A: Statistical Mechanics and its Application, vol. 316, no. 1, pp. 87-114, 2002.
[3] Bewick V. et al., Critical care, vol. 8, no. 6, p. 508, 2004.