#### **MECHANICAL ENGINEERING** TEXAS A&M UNIVERSITY

HUR (HUman Rehabilitation) Group

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# **Does Inadequate Angular Momentum Regulation Cause Falls?**



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# INTRODUCTION

#### Motivation

- Falls impact the economy negatively, costing over \$150 billion each year [1].
- Falls also negatively impact the society, by continually being amongst the top causes of the fatal injuries in the US work places [2].
- Sagittal angular momentum (H) is a quantity representing the movement of rotation of an object. Previous studies [3] indicated that severe slippers, who are more prone to fall [4], had significantly higher H following a slip, compared to mild slippers. The two severity groups also deviated in their COM height  $(COM_h)$ and Single/Double Stance duration (SS/DS) (Fig. 2)[3, 5].



Fig. 2: Average and Standard deviations tested Asterisk significant Heel the surface

# **Objectives**

To compare the time lead/lag between the deviations observed in  $COM_h$ , H, and single support duration to rule out or substantiate causal relationships.

## Hypotheses

### **Data Collection**

- Markers' data during normal walking were collected and slipping for analysis. Analysis
- COM<sub>h</sub> was calculated by weightedaveraging limbs' distances and masses.
- Severe slippers showed higher H postslipping (from 3% to 27%) (pvalue<0.001, Fig. 2b).
- Mild slippers had normal SS phase while all severe slippers had a shortened SS (p-value<0.001) and placed their swing limb on the floor

We hypothesize that a time-lead over COM<sub>h</sub> would substantiate a causal relationship between deviations in H and severe slipping, and hence, falling.

### METHODS

#### Subjects

Twenty healthy young adults (age  $(mean \pm SD) = 23.6 \pm 2.52)$  participated in this study upon signing a written consent. There were 11 males and 9 females and excluded in case of history of gait disorders.

#### Procedures

Participants were asked to walk at their comfortable speed in a long

- H was measured via multiplying each limb's mass, velocity, and angular velocity to its distance and moment of inertia, respectively, as it follows: H = $\sum_{i=1}^{n} m_i (r_{com/i} \times v_{com/i}) + I_i \omega_i$
- The gait cycle duration was normalized to 100 points for all subjects, and the slipping behavior was converted to 30 points (i.e. % gait cycle). The support duration analysis was done for 75% instead of 30% post-slipping (Fig. 2c). •  $COM_h$  and H were normalized to subject's weight, height, and speed.
- Subjects were classified as severe slippers if their Peak Heel Speed (PHS) during slipping exceeded 1.44 m/s [4].

after slipping ("toe-touch" behavior).

# **DISCUSSION and CONCLUSION**

• The time lead of the deviations in *H* over COM<sub>h</sub> suggests that the excessive rotation of the body, (i.e. higher H), causes the drop in COM<sub>b</sub> rather than a direct vertical collapse on the legs.

- Toe-touch could be a measure to constrain and lower H, since H can only be changed via a torque around the body's COM by the swing limb.
- *H* may be a key variable in controlling slips: The CNS may choose to change its control method and incorporate the

walkway. Subjects wore a harness system throughout the experiment. Subjects performed four "practice" walking trials" getting familiar with the setup. Then, a slippery contaminant was applied to the walkway without informing the subjects.



Independent t-test was used to find differences inter-group time and sequence of deviations examined.

#### RESULTS

Mild slippers (12 persons) and severe slippers (8 persons) were no different during the walking but were different in all tested variables upon slipping. Severity groups differed in COM<sub>h</sub> from 24% to 30% after slip initiation (pvalue<0.05, Fig. 2a).

toe-touch response as a measure to re-establish the balance, or even take a safer fall depending on how high H value is. Future studies should further investigate the causality of *H* to falls.

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#### References

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